

Reducing Clutter Noise in Fast Ultrasound Imaging with Transverse High-Pass Filtering

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Abstract – Clutter noise that appears as line strips in parallel with transducer surface is often seen in fast imaging with plane wave or waves of small divergences. In this paper, spatial high-pass filters of different cut-off frequencies are applied in the transverse direction in Fourier domain to reduce the clutter noise for the high-frame rate (HFR) imaging method developed previously. The noise reduction and contrast enhancement are significant when 11 transmissions (maximum frame rate of 413 frames/s at a speed of sound of 1500 m/s and 165-mm image depth) are used. However, with 91 transmissions (maximum frame rate of 50 frames/s), the method is less effective since the original image already has a low clutter noise and a high contrast.

Keywords - Clutter noise, high-frame-rate imaging, fast Fourier transform, plane wave imaging, and diverging beams

I. INTRODUCTION

Fast ultrasound imaging such as plane wave imaging [1]-[6] and imaging with waves of small divergences [7][8] is gaining a renewed interest in recent years due to the need of high image frame rate for elasticity imaging of moving objects [9]-[11], blood flow velocity vector imaging [12]-[15], and fast cardiac imaging [5][11][16]. However, due to a relatively flat wave front of the plane wave or waves that have small divergence angles [7][8], it is observed that there is clutter noise in images. The clutter noise appears as line strips that are generally in parallel with the surface of the transducer [1][2][4][5][7][17]. It is produced by imperfect receiver electronics [5][6][18], multiple reflections among parallel objects, and multiple reflections between the objects and the transducer surface. The clutter noise is most obvious in anechoic areas, at deeper depths where echo signals are weak and receiver gain is high, and the steering angle is small [4][5][7][17].

In this paper, the clutter noise is reduced with a spatial high-pass filter for the high-frame-rate (HFR) imaging method [1]-[8],[12][17]-[27] that was developed based on limited diffraction beams [13][14][28]-[35] and Fourier reconstruction. The filter is applied in the Fourier domain in a direction (transverse direction) that is in parallel with the transducer surface. Since the HFR imaging method is Fourier based, the application of the filter is straightforward [1][4][5].

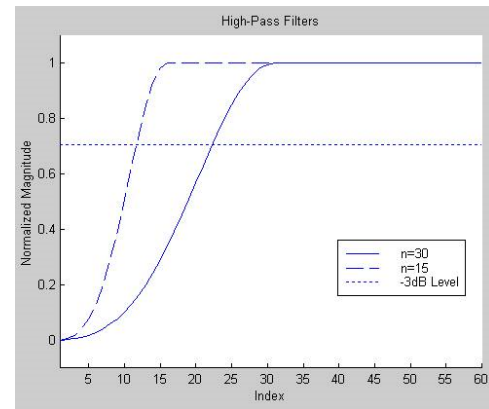


Figure 1. Transfer functions of the high-pass filters (they are an inverse of half of the Blackman window functions).

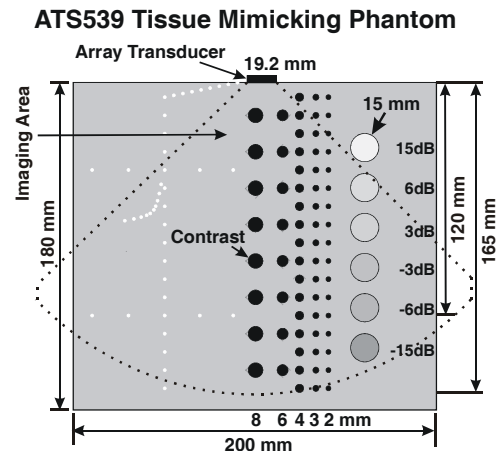


Figure 2. A cross-section of an ATS539 tissue-mimicking phantom showing the imaging areas of 120 mm and 165 mm depths with ± 45 degree field of view for the experiments. (Modified from Fig. 4 of [17].)

II. METHOD

In the study, two filters that have -3-dB cut-off frequencies of about 0.225 mm^{-1} and 0.45 mm^{-1} respectively were used ($\Delta k'_x = 0.02045 \text{ mm}^{-1}$ with a total number of points of 4096 and $\Delta x = 0.075 \text{ mm}$, where $\Delta k'_x$ and Δx are sampling intervals in the frequency and spatial domains of the image

respectively). The transfer functions of the filters have a shape of an inverted Blackman window (see Fig. 1) and the half widths of the windows of the two filters are $n=15$ and $n=30$ points (or spatial frequencies of 0.307 mm^{-1} and 0.614 mm^{-1}) respectively [36]. The filters were applied to all sub-images in the Fourier domain before a coherent superposition to form the final image from the sub-images using the HFR imaging method [1][4][5].

III. EXPERIMENT

Images of an ATS 539 tissue mimicking phantom (Fig. 2) were produced experimentally with plane waves and waves of small divergence angles in transmissions using a home-made HFR imaging system [5][6][18], and were reconstructed with the HFR imaging method developed previously based on the Fourier transformation [1][2]. In the experiment, a 128-element, 19.2-mm aperture, and 2.5-MHz linear array transducer of about 58% -6-dB pulse-echo fractional bandwidth was used.

Image Reconstruction with 11 Transmissions

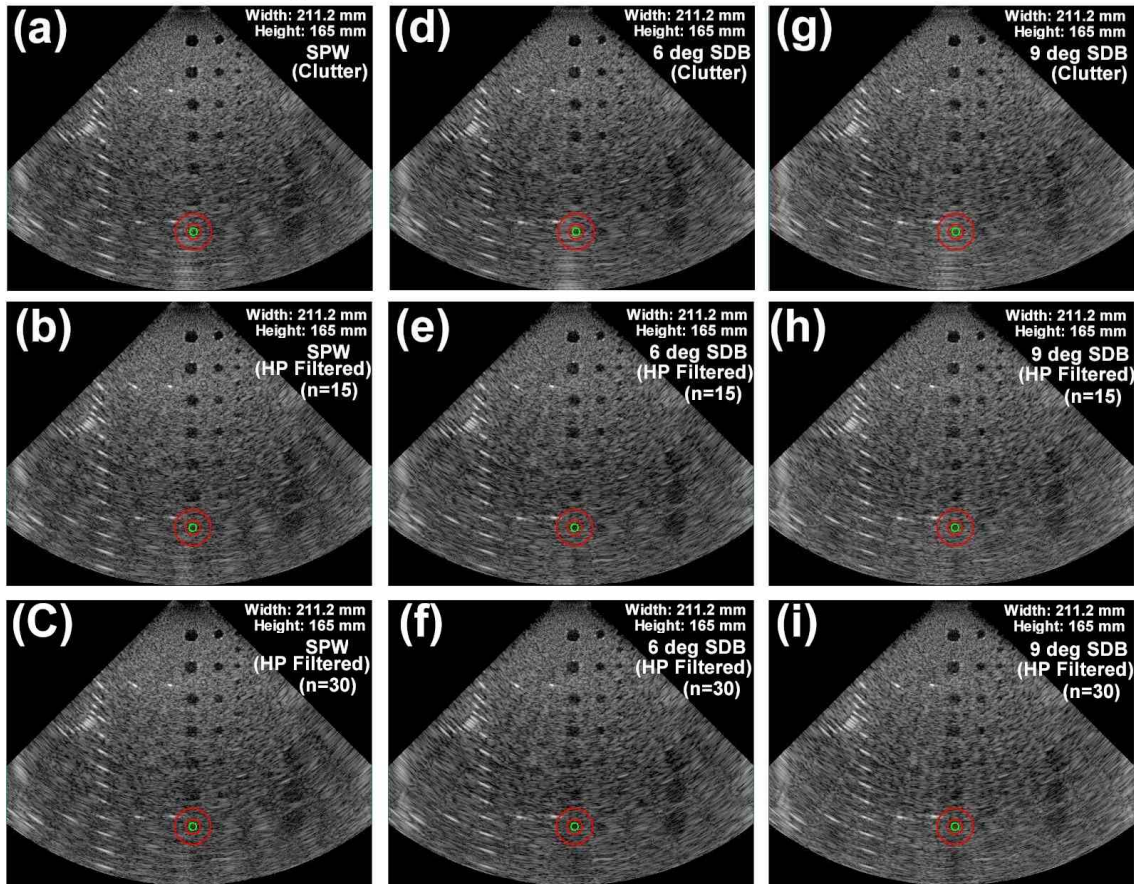


Figure 3. Effects of the high-pass filters on reduction of clutter noise (see areas around and below the red circles) for images reconstructed with the HFR imaging method with 11 transmissions and with echo signals acquired experimentally. 50 dB log compression has been applied.

IV. RESULTS

Fig. 3 and Fig. 4 show images reconstructed with the HFR imaging method with 11 (maximum frame rate of 413 frames/s at a speed of sound of 1500 m/s and 165-mm image depth) and 91 (maximum frame rate of 50 frames/s) transmissions respectively and with echo signals acquired experimentally. The images were obtained with steered plane wave (SPW) (first column), and steered diverging beams (SDB) of 6 (second column) and 9 (third column) degrees of

divergence angles. Images reconstructed with the clutter noise reduction (second and third rows for the high-pass filter with $n=15$ and $n=30$ points respectively) (see areas around and below the red circles) are compared with those without the noise reduction (first row). From Fig. 3, it is clear that with the high-pass filters, the clutter noise at deeper depths where the signals are weak is reduced and the contrasts of the cyst are increased for images reconstructed with 11 transmissions (this is the case for both SPW and SDB transmissions) (Table 1). As for images reconstructed

with 91 transmissions, their contrasts are slightly reduced after the clutter noise reduction (see Fig. 4 and Table 1). This means that the noise reduction method is more effective for fast image reconstruction where fewer transmissions are used

and is less effective for slower imaging that already has a higher image quality before the noise reduction.

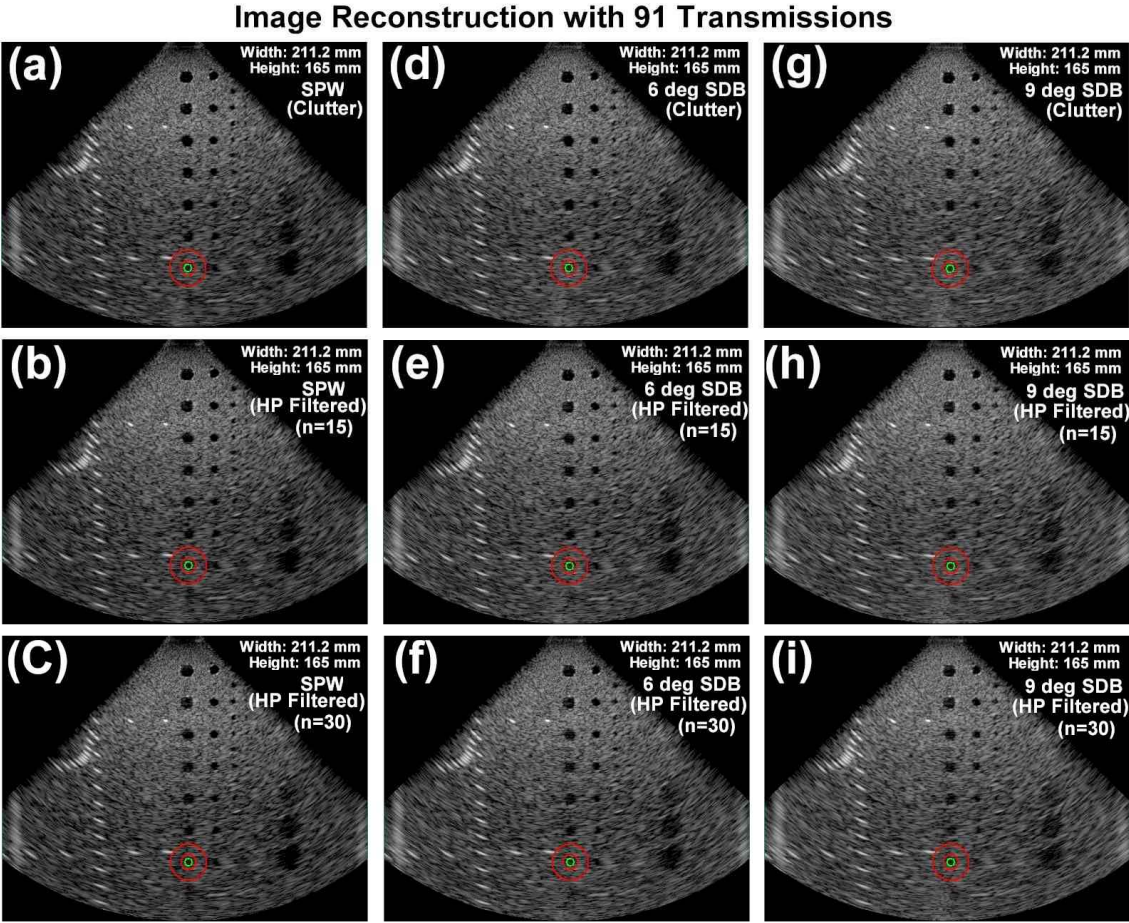


Figure 4. Effects of the high-pass filters on reduction of clutter noise (see areas around and below the red circles) for images reconstructed with the HFR imaging method with 91 transmissions and with echo signals acquired experimentally. 50 dB log compression has been applied.

Table 1. Contrasts (20 times the logarithm of the average pixel values inside the green circle over that between the two red rings) of the 7th large cyst (8 mm in diameter) from the top of the ATS539 tissue-mimicking phantom due to clutter noise reduction with high-pass filters (HPF) of different -3-dB cut-off spatial frequencies (0.225 mm^{-1} and 0.45 mm^{-1} for $n=15$ and $n=30$ respectively).

Cyst Contrast (dB)	11 Transmissions			91 Transmissions		
	SPW	SDB 6°	SDB 9°	SPW	SDB 6°	SDB 9°
No Filter	-2.32	-3.28	-3.16	-8.35	-7.29	-5.86
HPF (n=15)	-3.56	-5.64	-4.91	-7.93	-6.64	-5.73
HPF (n=30)	-3.30	-5.39	-4.35	-7.46	-6.64	-5.85

V. CONCLUSION

The clutter noise that appears as line strips in parallel with the surface of transducer is reduced significantly and image contrasts are increased greatly with high-pass filters for the HFR imaging of 11 transmissions. With a higher cut-off frequency, the clutter noise is further reduced but the image contrasts are also slightly reduced. With 91 transmissions, the effects of the filters are less effective since the original image already has a low clutter noise and high image contrast.

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